

Endoscopy in patients with implanted electronic devices

The ASGE Technology Committee provides reviews of existing, new, or emerging endoscopic technologies that have an impact on the practice of gastrointestinal endoscopy. Evidence-based methodology is used, with a MEDLINE literature search to identify pertinent clinical studies on the topic and a MAUDE (Food and Drug Administration Center for Devices and Radiological Health) database search to identify the reported complications of a given technology. Both are supplemented by accessing the "related articles" feature of PubMed and by scrutinizing pertinent references cited by the identified studies. Controlled clinical trials are emphasized, but in many cases data from randomized controlled trials are lacking. In such cases, large case series, preliminary clinical studies, and expert opinions are utilized. Technical data are gathered from traditional and Web-based publications, proprietary publications, and informal communications with pertinent vendors.

Technology Status Evaluation Reports are drafted by 1 or 2 members of the ASGE Technology Committee, reviewed and edited by the committee as a whole, and approved by the Governing Board of the ASGE. When financial guidance is indicated, the most recent coding data and list prices at the time of publication are provided. For this review, the MEDLINE database was searched through September 2006 for articles related to endoscopy in patients with implanted electronic devices by using the keywords "gastrointestinal endoscopy" and "electrocautery" paired with "pacemaker," "defibrillator," "ICD," and each of the miscellaneous noncardiac devices. In addition, this document also received review and contributions from physician representatives of the Heart Rhythm Society (Washington, DC).

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BACKGROUND

Endoscopy is commonly performed in patients with implanted electronic devices. Electrocautery is used in many endoscopic procedures. Endoscopists must be familiar with the potential for patient injury or interference with device function as a result of endoscopic intervention. This article will address the risks and the appropriate management strategies for endoscopy and the use of electrocautery in patients with implanted electronic devices, including the following: (1) cardiac devices (pacemakers and defibrillators), (2) neurostimulators (deep brain, gastric, spinal cord, sacral nerve, and urinary bladder stimulators), and (3) drug-infusion pumps (chemotherapy and pharmacotherapy infusion pumps) (Table 1). Other risks of GI endoscopy in patients with implanted electronic devices that are unrelated to electromagnetic interference are not addressed. Guidance regarding potential risks related to infection,¹ performance of wireless capsule endoscopy,² or wireless pH monitoring³ is available in other guidelines or technology evaluations.

TECHNICAL ISSUES

Electrocautery use during GI endoscopy

Electrocautery involves the application of radiofrequency current in a unipolar or bipolar/multipolar fashion to cut and/or coagulate tissues. In unipolar cautery, current passes from the active electrode of the electrosurgical device, through the patient to a distant return electrode (grounding pad), and back to the generator. During bipolar and multipolar cautery, current flows from 1 or more electrodes located on an electrosurgical device through immediately adjacent tissue and returns to 1 or more electrodes on the same instrument. During electrocautery, the resistance to flow of current generates heat, which enables electrocoagulation or electrosection (cutting effect). Coagulation occurs with short bursts of relatively low-energy current, whereas cutting uses continuous current generating high temperatures, which cause cell explosion and evaporation.⁴ Newer-generation electrosurgical generators use programmable blends of coagulation and cutting current.

The most common applications of monopolar cautery include the performance of endoscopic polypectomy (primarily in the colon or the stomach) and endoscopic sphincterotomy of the biliary or pancreatic sphincters at

TABLE 1. Device classes and devices

Device class	Device	Sensing capabilities	Patient controlled functions		
			On-off	Voltage or rate	Alter programming for electrocautery?
Cardiac					
	Pacemakers	Yes, most	No	No	Situational, see text
	ICD	Yes	No	No	Yes, with specialty input
Neurostimulators					
	DBS	No	Yes	No	See text
	GES	No	Yes	Yes	See text
	Other neurostimulators (spinal cord, peripheral nerve, urinary bladder, cochlear)	No	Most yes	Most yes	Yes
Medication delivery pumps					
	Pharmacologic agents (eg, narcotics, Lioresal, PGI ₂)	No	No	Most no	Most no
	Chemotherapeutic agents (floxuridine)	No	No	Most no	Most no

the major or minor papillae in the duodenum. “Hot biopsy” is a special form of polypectomy in which monopolar cautery is used to simultaneously coagulate and ablate the base of small polyps during sampling.⁵ Monopolar cautery is also used during the application of argon plasma coagulation for control of hemorrhage or for ablation of mucosal lesions, such as vascular malformations or residual polyp tissue.⁶ In this “noncontact” technique, the monopolar circuit is completed by passage of current via a stream of argon ions from the device tip to the tissue. In most monopolar applications, the duration of cautery is controlled by stepping on a foot pedal for the desired intervals of <1 second to 10 seconds or more.

Bipolar and multipolar cautery are used during direct application of “bicap” probes for control of local hemorrhage from ulcers or other vascular lesions.⁷ Power application can vary from brief pulses of <1 second to continuous application. The Olympus heat probe (Olympus Optical Co, Ltd, Tokyo) is a nonconductive hemostatic probe with a Teflon-coated tip that is heated by an internal electrical resistor. No current is passed through the tissues to either a local or distant electrode; hence, the induced electromagnetic field (EMF) (see below) is negligible.

Principles of electromagnetic interference

Electromagnetic interference (EMI) refers to the effect of an EMF on the function of any electronic device. EMI occurs as a result of 2 forms of EMF: conducted and radiated. Conducted EMI occurs when an electromagnetic

source comes in direct contact with the body (eg, electrocautery or defibrillation). Radiated EMI occurs when the body is placed in an EMF (eg, magnetic resonance imaging). Variables related to endoscopic or surgical electrocautery devices that determine the likelihood of interference with implanted devices include the intensity of the generated EMF, the frequency and waveform of the signal, the distance between the electrocautery application and the leads of the implanted device, and the orientation of the leads with respect to the EMF.⁸ Cutting current may be more likely to cause EMI than coagulation current.⁹ Because bipolar and multipolar devices induce only a limited flow of current beyond the site of application, a very localized EMF is generated and EMI is less likely compared with monopolar devices. Use of electrocautery can induce an EMF as high as 60 V/m. Variables that determine the sensitivity of an implanted device to an EMF include the presence and the number of leads, the distance between the anode and the cathode of the implanted device (smaller distance in bipolar leads vs unipolar leads), and the programmed sensitivity of the device to an electrical signal. Implanted devices that use bipolar sensing are less likely to experience EMI.¹⁰

Theoretically, EMI generated by an electrosurgical instrument on an implanted device can be manifested in the following ways¹⁰:

1. The signal may be interpreted as physiologic or pathophysiologic, temporarily inhibiting or triggering output.

- For example, the signal could be sensed as intrinsic cardiac electrical activity, with inhibition of a pacemakers output or as ventricular fibrillation (VF) resulting in discharge of an implantable cardioverter-defibrillator (ICD).
2. The signal may be interpreted as noise, temporarily or permanently causing the device to revert to a mode preset by the manufacturer.
 3. High levels of current may pass through the implanted leads and damage the contiguous tissue.
 4. A continuous train of electrical impulses may be conducted down the leads of an implanted device and cause inappropriate stimulation of the target tissue, such as ventricular or atrial fibrillation with pacemakers or ICDs.
 5. High levels of current may cause irreversible loss of battery power or permanent destruction of the device.

Because of the very different nature of the devices, cardiac devices, neurostimulators, drug-infusion pumps, and other devices will be considered separately in this report. For further discussion of EMI and the potential interaction with implanted cardiac devices, the reader is referred to recent reviews of the subject.¹¹⁻¹³ Situations 3, 4, and 5 above are very unlikely to occur in modern pacemakers and ICDs unless the current source is applied in very close proximity to the pulse generator or the lead electrodes, which is unlikely to occur in GI endoscopic procedures.

CARDIAC DEVICES

Two major classes of cardiac-rhythm-management devices are commonly used: pacemakers and ICDs. These devices have significantly different risks for abnormal function or injury and, hence, differing recommendations for their management during the use of electrocautery.

Cardiac pacemakers may be programmed in asynchronous modes (where the pacemaker paces but does not sense the atria or ventricle or both chambers) or synchronous modes (capable of sensing the atrial or ventricular impulse or both). All currently implanted pacemakers have programmable features (including, eg, control over pacing mode, rate, stimulus output, sensitivity, rate-responsiveness), the nature of which depends on the type of pacemaker used.¹⁴ The sensing thresholds of pacemakers (as low as 0.1 mV) are well below the EMFs induced by use of electrosurgical therapy, that is, electrosurgical current applied near pacemakers may be easily sensed as intrinsic cardiac electrical activity.¹⁵ Pacemakers are implanted in patients for a variety of indications, most commonly sinus-node dysfunction and atrioventricular (AV) block. The term “pacemaker dependent” is used to refer to patients who require cardiac pacing most or all of the time to maintain a physiologically adequate heart rate. This situation most commonly occurs in patients with a high-degree or a complete AV block.

ICDs successfully terminate VF in over 98% of episodes^{9,10} and have been shown to reduce mortality.¹¹ The indications for ICD use are expanding and now include not only patients with a history of ventricular arrhythmia but those found at risk because of left ventricular dysfunction.¹⁶⁻¹⁸ This device consists of a pulse generator and 1 or more leads for pacing and defibrillation electrodes. The pulse generator has a titanium case that houses a battery, voltage converters, capacitors, and other electronic capabilities of a pacemaker. Current ICD devices weigh 50 to 100 g, have a 30- to 70-mL volume, and are usually implanted in the anterior pectoral location, similar to a pacemaker.¹⁹ Some patients who have retained older epicardial or endocardial ICD systems or who have no upper-extremity venous access may have a generator implanted in the abdomen, usually in the left upper quadrant above the rectus muscle. Current-generation ICDs can perform all pacemaker functions, including bi-ventricular pacing; some patients with ICDs are also pacemaker dependent, usually because of concomitant AV block.

ICDs sense ventricular rate (R-R interval) by using a true or modified bipolar-sensing electrode, usually implanted on the endocardial surface of the right ventricle. ICDs detect ventricular tachyarrhythmias by sensing a number of R-R intervals above a rate threshold for a given duration, all these variables are programmable. Typical tachycardia detection criteria are rates higher than 150 to 200 bpm for 3 to 5 seconds. Ventricular tachycardia (VT) and VF events that meet detection criteria are treated by the delivery of antitachycardia pacing (ATP) for VT, countershocks for VT or VF, and antibradycardia pacing as needed for a short time after delivery of a counter shock. Patients may also use the antibradycardia pacing functions of the ICD chronically. The specific criteria for arrhythmia detection, cardioversion, and defibrillation vary between models and manufacturers, and are programmable.¹⁴ The signal caused by electrocautery is 1600 times greater than the sense threshold of the ICD and, hence, can be detected as VT or VF by ICDs if the signal is sufficiently close to the sensing electrode and prolonged to meet programmed detection criteria (D. Ruzin, Medtronic Inc, written communication, October, 2005).

Safety issues with cardiac devices

Published data regarding safety of endoscopic electrocautery use in patients with implanted cardiac pacemakers are limited and anecdotal. Two case series with limited numbers of procedures report safe use of electrocautery, without specific precautions during endoscopy in patients with pacemakers.^{20,21} Serious adverse events related to the endoscopic application of electrocautery in patients with pacemakers have not been reported.

Adverse events occurring during the use of intraoperative electrocautery in patients with a pacemaker have

decreased as a consequence of the increasing use of bipolar leads and improved pacemaker design, but they still occur.²²⁻²⁹ Reports of intracardiac device malfunction in this setting include pacing inhibition, pacing triggering, automatic mode switching, spurious tachyarrhythmia detection,³⁰ electrical reset,^{11,12} myocardial burns,¹³ VF,³¹ the runaway pacemaker syndrome,²⁴ and irreversible loss of output.³² Although the likelihood is low, transient pacemaker inhibition during actual delivery of electrocautery could occur, with resulting severe bradycardia or asystole in patients dependent on a pacemaker.

In theory, electrosurgical cautery in patients with ICDs could elicit inappropriate countershocks by the pulse generator, ATP, suspension of arrhythmia detection, or permanent damage/malfunction of the implanted device. However, there are no published reports of these events during endoscopy or surgery. The absence of such reports may be because of a general practice of temporarily inactivating ICDs during procedures in which electrocautery is used. Two series report experience with electrosurgical devices in a total of 4 dogs and 48 patients. There was uniform absence of sensing of the electrosurgical signal or ICD charging, reprogramming, malfunction, or damage.^{33,34} Despite the lack of reported events because of EMI, the potential risks of electrocautery should be considered in patients with ICDs undergoing an endoscopy and appropriate precautions taken.

Management of patients with cardiac devices

Because of limited available data on the safety and effectiveness of different strategies for cardiac-device management during endoscopy, as well as different features available in different cardiac-device makes and models, universal recommendations applying to all patients in all practice settings cannot be made at the present time. A *Practice Advisory for the Perioperative Management of Patients with Cardiac Rhythm Management Devices*,³⁵ based upon a survey by the American Society of Anesthesiology (ASA), provides a useful review of the subject even though few points of broad consensus were achieved.

Manufacturers' Web sites and device-specific literature are helpful sources of guidance regarding interventions in patients with implanted devices. Manufacturers' recommendations are often based on anecdotal case series and reports of pacemaker malfunction during surgery but not during GI endoscopy specifically. In the absence of data, the theoretical risk for significant morbidity led some manufacturers to issue recommendations that electrocautery or other therapies that generate EMFs should be avoided whenever possible in patients with implanted devices. At the present time, the preponderance of data support the safe use of electrocautery in patients who have pacemakers and ICDs, with proper precautions.

For patients with either pacemakers or ICDs, perioperative planning should include obtaining information on

the cardiac device make, model, type (eg, single chamber, dual chamber, biventricular), indication for the device, degree of pacemaker dependence, and the patient's underlying heart rhythm. For those with an ICD, a history of device utilization to treat VT and VF is also useful. Such patients are usually followed at regular intervals (every 3-6 months) in specialized device clinics and/or by heart rhythm specialists trained in device management. The patient's cardiology provider should be able to provide these data, as well as information regarding how the patient's device will respond to a magnet and advice regarding whether and how the patient's device should be reprogrammed during the procedure.

Pacemaker interrogation and reprogramming immediately before and after the procedure allows control over the pacemaker rate but is not always feasible in all practice settings and clinical situations because of a lack of availability of qualified personnel to perform this task. In some practice settings, transtelephonic monitoring may be performed to check basic pacemaker function. Internet-based home monitoring of some ICDs has recently become available. In the future, similar monitoring of pacemaker and ICD function in the postprocedure setting may be possible.

Patients who are pacemaker dependent patients (ie, those with complete AV block) and are undergoing endoscopy in which prolonged electrocautery (especially unipolar) is anticipated may require temporary (via magnet application) or permanent reprogramming of the pacemaker to an asynchronous mode (VOO or DOO). In general, a magnet held or taped in the proper position over a pacemaker generator will result in asynchronous pacing at a constant rate prespecified by the manufacturer (generally 70 to 100 bpm). The principal advantage of magnet application is ease of use and reversibility of the intervention. One disadvantage is that pacemakers with magnet rates near 100 bpm may not be well tolerated by some patients at rest. The magnet response varies among manufacturers and device models.

Most patients with modern pacemaker systems who are not pacemaker dependent (ie, patients with infrequent symptoms because of intermittent sinus-node dysfunction) will not require temporary or permanent pacemaker reprogramming for endoscopic procedures. Indeed, some patients with normal intrinsic heart rhythm will become symptomatic if programmed to asynchronous pacing mode, because of palpitations or diminution of cardiac output. In addition, although extremely rare, the potential for asynchronous-pacing-induced proarrhythmia is present. If pacemaker reprogramming is not performed, operators should be prepared to recognize and manage infrequent responses to electrocautery, such as ventricular pacing at the upper rate limit (because of rate-responsive behavior or ventricular tracking of sensed signal on the atrial channel), mode switching, and noise reversion to an asynchronous pacing mode. In general, these

responses, if they occur, will be transient and limited to the period during which electrocautery is applied.

For patients with ICDs, a principal concern regarding the use of electrocautery is the potential for triggering inappropriate ICD therapy. Inappropriate ATP during sinus rhythm may induce VT or VF in a susceptible patient. ICD discharges, especially repetitive discharges in an awake patient, may be psychologically traumatic, may induce arrhythmia or cause hemodynamic instability, and may cause physical injury because of sudden muscle contraction or reactive patient movement during a delicate procedure. Although such adverse events have not been reported in patients undergoing endoscopy, the potential for such events nonetheless exists and may be underreported. Furthermore, the absence of reported adverse events may also be because of the widespread practice of temporary ICD inactivation for such procedures.

A magnet properly applied over the pulse generator of most ICD models will result in suspension of tachycardia detection and/or ICD therapies, while the magnet is in place, without affecting pacemaker function. Although magnet use is attractive because of its simplicity and ease of reversibility, there are several limitations to the approach of magnet application in this setting:

1. In some ICD models made by 1 manufacturer (Guidant Corp, St. Paul, Minn), the ICD response to a magnet can be programmed by prolonged magnet application to either permanently disable ICD therapies, temporarily disable ICD therapies while the magnet is in place, or to ignore a magnet entirely. For these devices, one cannot know how these devices will respond to a magnet without knowing how this feature is programmed. The potential to permanently inactivate ICD therapies with a magnet exists with these devices, with at least 2 documented sudden death.³⁶
2. Unlike a pacemaker response to a magnet, where asynchronous pacing can be easily observed, it is more difficult to ascertain whether the magnet is properly positioned over an ICD. The proper position varies among different device manufacturers and models, and while some devices emit a tone when a magnet is placed properly, others provide no feedback to prove proper placement.
3. Even if initially placed properly, a magnet may move out of place during the procedure, especially if patient repositioning is required. In part for these reasons, the 2005 ASA Practice Advisory "cautions against the use of a magnet over an ICD."³⁵ It should be recognized, however, that alternative approaches also have limitations and that no adverse events from magnet use during endoscopy have been reported. Furthermore, some endoscopy facilities with proper training, experience, and heart rhythm specialty support have a long record of using magnets for this purpose, without adverse events.

ICD interrogation and reprogramming to suspend tachycardia detection and/or therapies have been recommended as the optimal solution to prevent the potential risk of inappropriate ICD therapies during use of electrocautery.³⁷ One limitation of this approach is the need to have qualified personnel available to perform the task immediately before and after the procedure. During this period of inactivation, Patients with an ICD are not protected by the device and, hence, must be monitored continuously in a setting where VT/VF can be immediately recognized and treated with external defibrillation. If external defibrillation is required, attempts should be made to avoid placing the external defibrillator pads or paddles directly over the ICD generator, but immediate resuscitation of the patient should be the first consideration. Finally, endoscopy facilities that use an approach of ICD reprogramming should establish a fail-safe protocol for ensuring that, in patients with an ICD, the ICD is appropriately reprogrammed after the procedure and that no patient ever leaves the monitored setting with the ICD inappropriately inactivated. Several patient deaths from VT/VF have been documented because of this preventable medical error.³⁸

The patient with the ICD who is also dependent on the pacemaker function of the ICD represents a particular challenge, because magnets do not affect the pacing function of most ICDs, and many ICDs cannot be programmed to an asynchronous pacing mode because of manufacturer concerns about interference with VT/VF detection. Accordingly, particular care should be taken with electrocautery in these patients, and preprocedure consultation with a cardiologist or a heart-rhythm specialist may be advisable.

Summary recommendations for cardiac devices

By recognizing that the paucity of published clinical data favoring any given approach, that the availability of heart rhythm specialty support varies by geographic region and practice setting, and that the variation in practice currently exists in this area, the following general recommendations are made to minimize the risks to patients with implanted cardiac devices who are undergoing endoscopic procedures that require the use of electrocautery.

- In all patients with implanted cardiac devices.
 - Determine the type of cardiac device, indication for the device, the patient's underlying cardiac rhythm, and degree of pacemaker-dependence before endoscopy. Most patients carry wallet cards that identify the device make and model, with manufacturer contact numbers. Contacting the patient's cardiologist or heart rhythm specialist and/or the device manufacturer may be helpful, especially in concert with the evaluation by an on-site heart rhythm specialist or device nurse.
 - Use continuous electrocardiographic rhythm monitoring in addition to pulse oximetry during the procedure.

- Have appropriate equipment for resuscitation, cardioversion, and defibrillation immediately available. This should include an external defibrillator with transcutaneous pacing capability.
- Consider the use of endoscopic devices with limited or no EMF (such as noncautery thermal probes or bipolar/multipolar probes).
- Use the lowest effective power output and the briefest application of the electrocautery device possible.
- Place grounding pads a good distance from the pulse generator and leads, such that the implanted device and leads are not between the cautery source and the grounding pad.
- Avoid use of cautery near implanted devices (Some investigators advise avoiding therapy within 15 cm).
- Most patients with cardiac pacemakers may undergo routine uses of electrocautery (eg, polypectomy, hemostasis) with no alterations in management.
- For patients who are pacemaker dependent and in whom prolonged electrocautery is anticipated (eg, treatment of gastric antral vascular ectasia or radiation proctitis) consider reprogramming the pacemaker to an asynchronous mode via application of a magnet over the pulse generator during the use of electrocautery.
- For patients with an ICD in whom the use of any electrocautery may be anticipated, consultation with a cardiologist or a heart-rhythm specialist is recommended. Deactivation of the ICD function by qualified personnel should be considered. Continuous rhythm monitoring should be used throughout the interval that the ICD is deactivated. If deactivated, the ICD should be reprogrammed as soon as possible after the procedure and before cessation of monitoring or dismissal.
- If the patient with an ICD is also pacemaker dependent and the ICD cannot be reprogrammed to an asynchronous mode and prolonged cautery application may be required, then strongly consider the use of bipolar cautery or a device with no EMF.

NEUROSTIMULATORY DEVICES

Neurostimulators are implantable devices that deliver electrical stimulation to selected tissues, such as the brain, spinal cord, neural plexuses, gastric serosa, urinary bladder, cochlea, and potentially other end organs. The devices generally consist of an electrical source, extension wires, and 1 or more leads that deliver the electrical stimulus. Most of the neurostimulatory devices have simple external modules for patient control of various settings, including the “on-off” function and voltage output.

The deep brain stimulator (DBS) (Activa Control Therapy; Medtronic, Inc, Minneapolis, Minn)³⁹ delivers electrical stimulation to selected areas of the brain for control of aberrant brain signals in the management of Parkinson’s disease and other movement disorders. By 2004, more

than 14,000 implants had been performed worldwide³⁹; however, there is a potential for increasing use, because the annual incidence of Parkinson’s disease ranges from 500,000 to 1 million people in the United States.⁴⁰ The DBS measures 61 × 76 × 13.4 mm, weighs 83 g, and is housed in a titanium-alloy body. The device electrodes are stereotactically placed in various areas of the brain. The lead is tunneled subcutaneously down the side of the skull where it meets the extension wire just behind the ear. The extension is then tunneled down the neck and into the anterior chest-wall location, where it is connected to the neurostimulator. The patient can activate and deactivate the neurostimulator by placing a magnet on the overlying skin. The DBS also provides telemetry data and can be set in either a unipolar or bipolar configuration.

The gastric electrical stimulation (GES) system (Enterra Therapy; Medtronic) is indicated for stimulation of gastric motility in the treatment of patients with chronic, intractable (drug refractory) nausea, and vomiting secondary to gastroparesis of either diabetic or idiopathic etiology. It was approved by the Food and Drug Administration, with a humanitarian-device exemption in 2000.⁴¹ An evolving indication in the literature is its possible use for morbid obesity. The device has a programmable battery-operated neurostimulator⁴² that weighs 42 g and measures 55 × 60 × 10 mm. Single or dual leads are tunneled subcutaneously from the neurostimulator in the anterior abdominal wall to the gastric serosal surface where unipolar or multipolar function stimulation is delivered.

Other neurostimulation devices (peripheral nerve, spinal-cord stimulators, urinary bladder, and cochlear) are similar in principals and have similar designs.

IMPLANTED INFUSION PUMPS

Implanted infusion pumps are indicated when therapy involves the constant, chronic intrathecal, epidural, or intravascular infusion of pharmacologic agents (eg, narcotic, floxuridine, baclofen, and prostaglandin I₂ [PGI₂]). These implantable devices store and dispense drugs at a constant flow rate set during the manufacturing process or a programmable rate that can be set by the physician. Programmable pumps are battery powered, whereas constant-flow pumps have a propellant chamber. Both have a pump drive and a central reservoir fill port. Certain models have an optional catheter-access port that is used for diagnostic purposes.

Safety issues in patients with neurostimulators and infusion pumps

Safety data are almost nonexistent for the recently developed neurologic and gastric stimulators and infusion pumps. One report described the development of left-sided paresthesias in a patient with a DBS who underwent

repeated dermatologic surgery by using monopolar electrocautery with or without the use of a dispersive plate. With the use of a battery-operated cautery device the symptoms did not recur.⁴³ Another case reported the use of a battery-operated electrocautery device, without production of neurologic symptoms in a patient with a DBS.⁴⁴ A survey of the Maude database revealed 1 case report of DBS where a patient was “shocked” during the use of monopolar electrocautery.⁴⁵

Industry guidance and device inserts for the Activa DBS, Enterra GES Systems suggest that electrocautery can cause the following: (1) temporary neurostimulator device malfunction that presents as suppression of output and/or reprogramming to reset parameters; (2) induced currents within leads, yielding symptoms of shocking or jolting and potential injury; and (3) electrode heating, with a risk of focal tissue injury (Mr Curt Sponberg, Safety Representative, Medtronic Inc, personal written communication, August, 2006).^{46,47}

Permanent malfunction from electrocautery is unexpected, and temporary malfunction can be mitigated by turning off the device during the procedure in which electrocautery will be used. Induced currents in implanted leads may develop whether the device is turned on or off. The level of EMFs necessary to cause a malfunction or induced currents has not been determined. Electrode heating may be mitigated by limiting contact currents to <6 mA for 10 seconds or 18 mA for 1 second (C. Sponberg, personal communication). Correlation of these levels to outputs of clinical devices has not been investigated.

There is also no published literature regarding the safe use of electrocautery in patients with implanted infusion pumps. The manufacturer’s *System Components Clinical Reference Manual* states the following. “Testing indicates electrocautery is unlikely to damage the pump; however, if electrocautery is necessary near the pump, then follow these precautions: (1) use only bipolar cautery, and (2) if unipolar cautery is necessary, then do not use high-voltage modes, keep the power settings as low as possible, and keep the current path (ground plate) as far away from the pump and catheter as possible.”⁴⁸

Recommendations for the use of electrocautery in patients with any of the noncardiac devices are based upon principles similar to those for cardiac devices, as well as on manufacturers’ guidance (Table 1). As with cardiac devices, guidance should be sought from both manufacturers and the physician specialist managing the device application for the given patient. In general, the neurostimulators for regions outside of the central nervous system, particularly those involving the spinal cord and peripheral nerves or organs, can be reduced to zero voltage output and then shut off entirely. Some devices can be inactivated but cannot be adjusted downward to zero. Specialty physician input should be sought before inactivating the DBS or the GES system.

Summary recommendations for noncardiac devices

The type of electronic device, the indication for the device, and whether normal physiology is critically dependent upon the device should be determined. Most patients carry wallet cards that identify the device make and model, with manufacturer contact numbers. Contacting the patient’s device specialist and/or the manufacturer may be helpful in planning device management during and after the procedure.

- Consider the use of endoscopic devices with limited or no EMF (such as noncautery thermal probes or bipolar/multipolar probes).
- Use the lowest effective power output and the briefest application of the electrocautery device possible.
- Place grounding pads a good distance from the device’s generator and leads, so that the implanted device and leads are not between the cautery source and the grounding pad.
- Avoid the use of cautery near implanted devices.
- For patients with DBS and GES devices, consult the primary device specialist before considering inactivation of the device output.
- For patients with spinal cord and most other peripheral neurologic stimulation devices, have the patient zero the voltage output and then turn off the device before use of electrocautery.

CONCLUSIONS

Implanted electronic devices are increasingly encountered during GI endoscopy. Endoscopists must be aware of the risks for patient injury and device damage or malfunction and must take precautionary steps to minimize the risk for their patients. The published data are quite limited. Further studies should address the risk of adverse events related to electromagnetic interference during GI endoscopy.

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This document is a product of the Technology Assessment Committee. The document was reviewed and approved by the Governing Board of the American Society for Gastrointestinal Endoscopy.